

The Design of Polyelectrolyte Multilayers Using Galactosylated Chitosan

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ABSTRACT

A major challenge in hepatic tissue engineering is that liver cells rapidly lose their phenotype in *in vitro* cell culture systems. For this reason, it is necessary to design biomaterials that can support and enhance hepatic functions. Hepatocytes have a surface protein, called the asialoglycoprotein receptor (ASGP-R), which interacts with galactose via a specific receptor-ligand interaction. Polyelectrolyte multilayers (PEMs) were prepared by the layer by layer method, which is based on electrostatic attractions between oppositely charged polyelectrolytes (PEs). Anionic (hyaluronic acid) and cationic (chitosan and galactosylated chitosan) PEs were used in the fabrication of detachable, free-standing PEMs. The main focus of this study is the design of PEMs comprised of 50 bilayers of PEs. PEMs that contained galactose functional groups were assembled with either 5 or 10 bilayers of galactosylated chitosan (5 - 10 % of galactosylation). Optical properties, solvent stability and surface topography of the PEMs were measured.

For my Family

Oktay, Nurcan, Özlem and Çağla ARCA

For your unconditional Love

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List of Abbreviations

ASGP-R: Asialoglycoprotein Receptor

BL: Bilayer

CS: Chitosan

EDC: 1-Ethyl-3-(3-dimethylaminopropyl) carbodiimide

GA: Glutaraldehyde

Gal-CS: Galactosylated chitosan

HA: Hyaluronic acid

LA: Lactobionic Acid

NHS: N-Hydroxysuccinimide

PE: Polyelectrolyte

PEMs: Polyelectrolyte Multilayers

Chapter 1: Introduction and Background

1.1 Introduction to Polyelectrolyte Multilayers (PEMs)

PEMs were pioneered by Decher et al. in 1990s [1, 2] and their fabrication is based on the layer by layer method of oppositely charged PEs. As a result of the alternating adsorption of anionic and cationic PEs, self-assembled multilayers can be formed. PEMs have been used in a wide range of applications such as drug delivery [3, 4], tissue engineering [5, 6], anti-viral coatings [7, 8] and microelectronics [9].

1.1.1 Layer by Layer Method and Parameters Effecting Properties of PEMs

PEMs can be prepared either by dipping or spraying methods. In the dipping method, substrates are immersed into PE solutions and after the deposition of a PE, PEMs are dipped into washing solutions. The PEMs can be coated either on 2D surfaces [10, 11] or on 3D structures such as fibers [12, 13], microparticles or wafers [14]. In the spraying method, PEMs are prepared by spraying PE solutions onto substrates and rinsing thereafter. This accelerates the assembly time of PEMs drastically (500 times) and such multilayers are much thinner than those prepared by the dipping technique (about 70-75% less) [15].

When a solid substrate is immersed into a negatively charged PE (Polymer A) solution, a monolayer of Polymer A is deposited on the substrate and the surface becomes negatively charged. After rinsing in water, the substrate is then immersed into the positively charged PE solution (Polymer B) and a thin monolayer of Polymer B is deposited. It usually takes a couple of cycles of deposition before the surface is completely covered by the PEs [16, 17]. By repeating these steps in an alternating manner, a self-assembled multilayer is obtained which

contains both PEs [2]. Polymer concentration, molecular weight, deposition time and ionic strength [18] have influence on the thickness of PEMs [19]. Since the assembly depends on electrostatic interactions, the PEMs can be also modified by varying the pH [20], the number of bilayers [17] and the first (anchoring) layer of the multi-layer assembly [21]. Apart from these parameters, properties of PEMs can be changed by post-modification such as cross-linking [10] or addition of functional groups [22]. The differences in the fabrication of PEMs and post-modification methods will change its properties such as swelling, thickness, stiffness or optical properties.

1.1.1.1 The Effect of Salt Concentration

The adsorption of the oppositely charged PEs is an ion exchange phenomenon. The surface charge of PEs can be compensated by salt ions. At low salt concentration, PEs are very efficient in assembling on the charged substrate surface but as the salt concentration increases, it prevents the charged polymer chains from being attached to the substrate. If the salt concentration is equal to the critical salt ion concentration, the salt ions will prevent the polymer assembly on the substrate [19, 23-25].

1.1.1.2 pH Effect

The dissociation of functional groups in a PE is a property dependent on the pH of the solution. If the pH of the solution is close to the pKa value, the charge density of polymer chains decreases and this leads to the assembly of the polymer on the substrate as a thick layer and a loopy conformation [25]. This loopy conformation is not ionically cross-linked and therefore more susceptible to swelling which increases the permeability of the PEMs [26]. When there is a

difference in pH and pKa, the charge of the polymer chains decreases and this leads to the adsorption of thin rigid films [25].

1.1.1.3 The Effect of PE Structure and Dissociation Constant

The variation in the structure of the polymer can lead to different conformation of the polymer chains and thus change the property of PEMs. It is known that λ -carrageenan has the random coil conformation and ι -carrageenan has helical conformation [27]. Schoeler et al published that the film stiffness of PEMs assembled with ι -carrageenan is three times more than PEMs with λ -carrageenan [28].

The dissociation constants of PEs can influence the film thickness. Assembly of strong PEs will lead to a linear increase in the film thickness as a function of the number of bilayers [29] due to the high charge density along the backbone of the polymer, such as poly(styrene sulfonate)/poly(allylamine hydrochloride) [30] and poly(styrene sulfonate)/poly(diallyldimethylammonium) PEMs [31].

On the other hand, the thickness of weak PEs increases exponentially with the number of bilayers, such as hyaluronic acid (HA)/poly(L-lysine) (PLL) [32, 33] and HA/chitosan (CS) PEMs [34]. This exponential increase depends on the diffusion of the polymer chains in and out of the assembled PEMs during each PE deposition step. Picart et al, demonstrated the exponential increase in film thickness in HA/PLL PEMs [32].

1.2 Introduction to Liver

1.2.1 Liver Organization and Function

The liver is divided into lobules and each lobule consists of plates of hepatocytes lined by sinusoidal capillaries. The blood supply brings many different types of endobiotics (hormones, proteins, and signaling molecules), xenobiotics (drugs, ethanol) as well as nutrients and oxygen to the liver. The liver is responsible for the detoxification of harmful substances, metabolism of amino acids, carbohydrates and lipids, and fat soluble vitamins such as vitamin A [35] and vitamin D [36], synthesis of plasma proteins such as albumin, globulin, fibrinogen, prothrombin, and antithrombin and, production of bile acids to aid fat digestion and absorption [37]. In addition, the liver takes part in the immune response in order to defend the body against pathogens such as bacteria [38]. It also converts hydrophobic substances into water soluble materials via enzymes in the endoplasmic reticulum to prevent an accumulation of lipid-soluble exogenous and endogenous compounds that are subsequently be excreted by the kidney [39]. The liver also takes part in the destruction of erythrocytes [40].

Sinusoidal cells constitute 33 % of the liver cells, which are endothelial cells (around 70% of the sinusoidal cells), Kupffer cells (liver macrophages, around 20%), fat-storing cells (stellate cells or Ito cells, around 10%) and pit cells (natural killer cells, < 1 %). Hepatocytes comprise the remaining cells [41].

1.2.2 Hepatocyte Membrane Protein: Asialoglycoprotein Receptor

ASGP-R is a calcium ion dependent [42] membrane protein, which is specific to mammalian hepatocytes. Ashwell and Morell first reported in the 1960s that glycoproteins with terminal

galactose or N-acetylgalactosamine residues are removed from the circulation *in vivo* [43]. The study was extended with the identification of liver plasma membranes as the primary binding site of asialoglycoproteins and this interaction was also shown in *in vitro* studies [44]. Pricer and Ashwell specified that the ASGP-R binding to the glycoprotein required the removal of sialic acid residues and the presence of a substituent on the plasma protein [44].

ASGP-R plays a role in the endocytosis via the clathrin coated pit pathway and degradation of a variety of desialylated glycoproteins and neoglycoproteins [45, 46]. ASGP-R binds and internalizes these asialoglycoprotein ligands via endocytic vesicles. After that, ligands are delivered to lysosomes for degradation and the receptors are recycled to the cell surface [47]. The receptors are available on the sinusoidal plasma membranes of the rat hepatocytes but not on the bile canalicular membrane [47, 48]. Hepatocytes isolated with sub-cellular fractionation of rat liver or detergent solubilization methods have about 90% of the receptors not on the cell surface but rather in Golgi, microsomal, and lysosomal membrane fractions and in segments of the endoplasmic reticulum, if asialoglycoproteins are available [49, 50]. The average number of receptors present on a cell (surface and interior) is approximately 4.5×10^5 [51].

1.3 Chitosan

CS is a deacetylated derivative of chitin and a binary heteropolysaccharide which consists of (1-4)-linked 2-acetamide-2-deoxy- β -D-glucopyranose and 2-amino-2-deoxy- β -D-glucopyranose residues [52] (**Figure 1.1**).

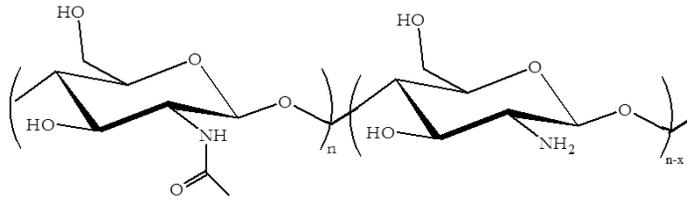


Figure 1.1 Structure of CS

Physicochemical properties of CS can change according to its molecular weight and extent of deacetylation. The degree of acetylation represents the mole fraction of acetylated units in the polymer chain, the proportion of N-acetyl-D-glucosamine units with respect to the total number of monomers. Generally, CS has a degree of deacetylation 50 % or above [53].

CS can degrade *in vivo* via enzymatic hydrolysis by lysozyme. It is insoluble in water and organic solvents but becomes soluble in dilute acidic solutions (pH < 6.0 - 6.5), when its primary amino groups become protonated. This renders the molecule positively charged [54, 55] and makes it a cationic PE. It precipitates in alkaline solution or forms gels with anionic PE at lower pH [56, 57]. Due to the cationic nature of CS, it can interact with anionic glycosaminoglycans, proteoglycans and other negatively charged molecules [55] such as HA [58]. It has the ability to form films [10, 59, 60] and can be used as a sponge, gel or microcapsules [58]. CS is a promising polymer for tissue engineering due to its favorable properties. These include CS being nontoxic, non-allergenic, antimicrobial, biocompatible and biodegradable [61-63]. It has structural similarity to glycosaminoglycans which are a major component of the extracellular matrix (ECM) [63], and stimulates attachment, proliferation and viability of cells including stem cells, and also the retention of cell morphology [55]. It is compatible with hepatocytes [64, 65]. Moreover, amino and hydroxyl groups of CS can be chemically modified with a variety of ligands.

1.4 Hyaluronic Acid

HA is a linear polysaccharide and an alternating copolymer of glucuronic acid and *N*-acetylglucosamine. It is a natural material with a high molecular weight (10^5 to 10^7 Dalton) and lacks immunogenicity. Its chemical composition (**Figure 1.2**) is identical for both humans and animals thus it can be isolated from rooster combs or streptococci cultures [66].

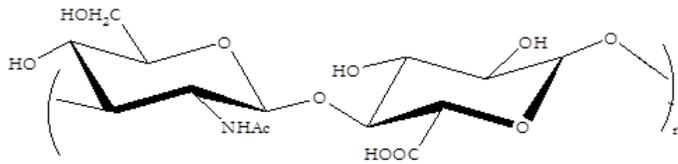


Figure 1.2 Structure of HA

HA is a component of the ECM in most tissues [67]. It is the only sulfate group free glycosaminoglycan and does not have a proteoglycan primer. Therefore it cannot form a proteoglycan. Its viscosity depends on the concentration, and this polysaccharide can form very viscous solutions but not a gel [68]. HA is a weak PE with good biocompatibility, nontoxicity, and biodegradability [69]. Due to these properties, it has been used in tissue engineering [70] and drug delivery [71].

Chapter 2. Synthesis of Galactosylated Chitosan and Accompanying Characterization

2.1 Introduction

Galactose is a 6C sugar that is a C-4 epimer of glucose. The structure of galactose is presented in **Figure 2.1**.

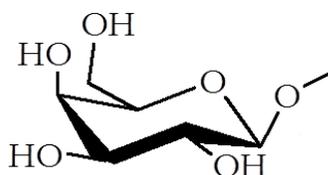


Figure 2.1 Structure of β -D-Galactopyranose

The free amino groups of CS are easily modified with the introduction of galactose group by carbodiimide chemistry. This chemical modification increases its bioactivity.

1-Ethyl-3-(3-dimethylaminopropyl) carbodiimide (EDC) is a favorable carbodiimide for use in conjugating biomaterials since it is water soluble and can be directly added to the reaction medium without the use of an organic solvent. The pH of the reaction medium typically ranges between 6.0-7.0 [72]. N-hydroxyl succinimide (NHS) esters are typically added to EDC reactions.

The introduction of galactose into CS results in galactosylated chitosan (Gal-CS) which can be further used as a scaffold biomaterial for hepatic tissue engineering. This has been successfully used to prepare cell culture substrates [73]. Adhesion of hepatocytes on galactosylated substrates are mediated by the galactose-specific interactions between ASGP-R of the hepatocytes and galactose residues present on the surface of the substrates [74, 75].

2.2 Materials and Methods

2.2.1 Materials

Medium molecular weight CS (≈ 350 kDa), N-Hydroxysuccinimide (NHS) and deuterium oxide (D_2O) were obtained from Sigma-Aldrich (St. Louis, MO). 1-Ethyl-3-(3-dimethylaminopropyl) carbodiimide (EDC), lactobionic acid (LA), trifluoroacetic acid-d (CF_3COOD), acetic acid (CH_3COOH) and acetone were received from Fischer Scientific (Pittsburgh, PA). Dialysis membranes were obtained from Spectrum Laboratories (Rancho Dominguez, CA) with a MWCO 3500.

2.2.2 Calculation of the Extent of Acetylation in CS

Deacetylation degree of CS was calculated by 1H -NMR of 10 samples from the same batch of CS. 0.005 g Gal-CS was dissolved in 1 ml D_2O and 10 μl CF_3COOD solution. The solution was mixed for 3 hours and then transferred to NMR tubes for analysis. 1H -NMR spectra were measured using INOVA 400 spectrometer, (VARIAN, Palo Alto, CA). The proportion of N-acetyl-D-glucosamine units with respect to the total number of monomers was calculated by using the integral intensity proportions of $-CH_3$ peak of acetyl group of CS, and the sum of integral intensities, H_2 , H_3 , H_4 , H_5 , H_6 , and H_6' protons.

2.2.3 Synthesis and Purification of Gal-CS

Galactose-containing LA was covalently coupled with CS using carbodiimide chemistry. Briefly, 0.44 g CS was added to 30 ml deionized (DI) water with 200 μl of acetic acid. This solution was stirred until the polymer was dissolved and a clear solution was obtained. In another beaker, 0.44 g LA, 0.035 g NHS and 0.12 g EDC were dissolved in 2 ml DI water. Then

this solution was carefully added to the CS solution. After 15 min, the pH was measured. The reaction was stirred at room temperature for 3 days.

Table 2.1 Syntheses for Different Extents of Galactosylation

Percentage of galactosylation	CS (g)	LA (g)	NHS (g)	EDC (g)	pH
5 %	0.44	0.44	0.035	0.12	5.7-6.0
10 %	0.44	0.88	0.07	0.24	5.7-6.0
15 %	0.44	1.25	0.10	0.36	5.7-6.0

After the synthesis, the polymer was purified by dialysis for 4 days against distilled water, precipitated with acetone and then dried at room temperature overnight.

2.2.4 ¹H-NMR Measurements

0.005 g Gal-CS was dissolved in 1 ml D₂O and 10 μl CF₃COOD. The solution was mixed for 3 hours and then transferred to NMR tubes for analysis. ¹H-NMR spectra were measured on an INOVA 400 spectrometer, (VARIAN, Palo Alto, CA).

2.2.5 FTIR Sample Preparation and Measurement

After precipitation with acetone, the polymer was placed on a p-tetrafluoroethylene (PTFE) substrate and dried at room temperature. FTIR spectra were obtained on a M series FTIR spectrometer (MIDAC Corporation, Westfield, MA).

2.3 Results

The method Hirai et al [76] developed was used to calculate the degree of deacetylation of CS by using the integral intensity proportions of acetyl groups and the sum of integral intensities, H₂, H₃, H₄, H₅, H₆, and H_{6'} protons (**Figure 2.2**) in a ¹H-NMR spectrum.

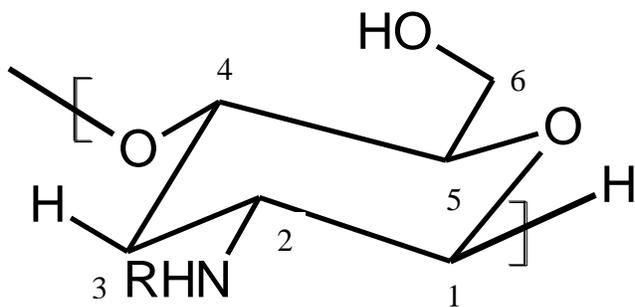


Figure 2.2 CS Structure to Show the Proton Numbers

The formula used to calculate the degree of acetylation of CS:

$$\text{Acetylation degree} = \frac{\frac{1}{3} (I_{\text{CH}_3})}{\frac{1}{6} (I_{\text{H}_2-\text{H}_6})} \times 100$$

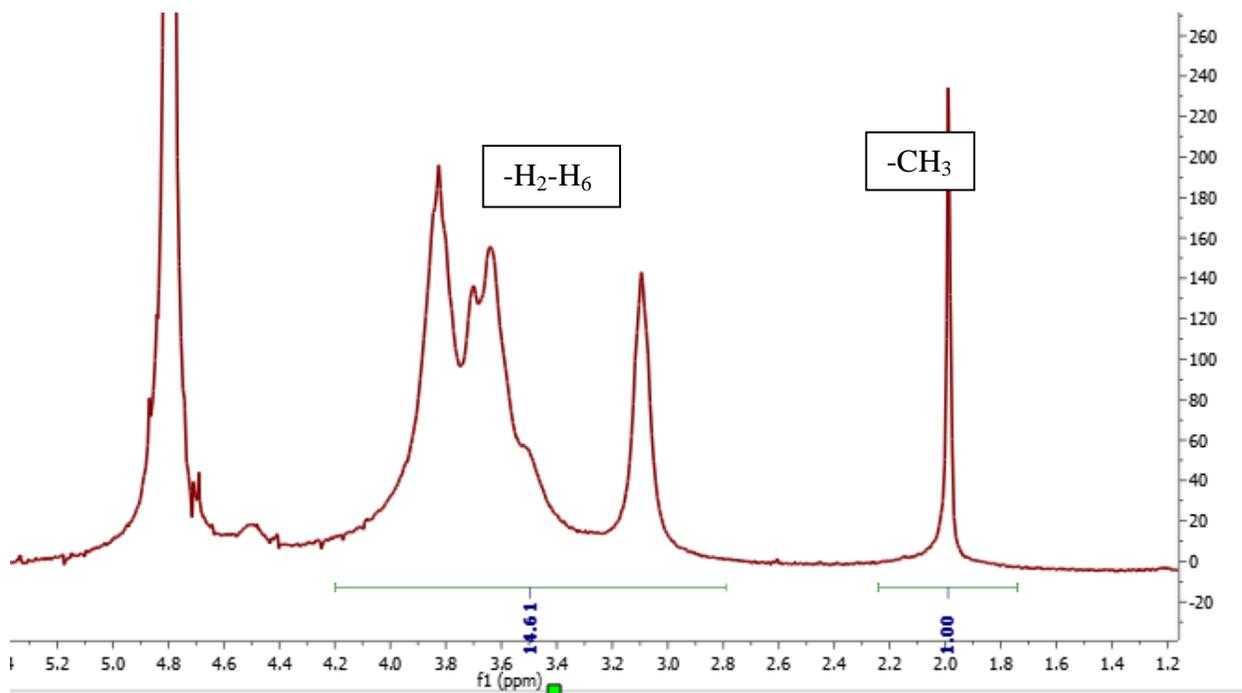


Figure 2.3 400 MHz ¹H NMR spectrum of CS in CF₃COOD/D₂O

In **Figure 2.3**, the intensity of the $-\text{CH}_3$ peak is 1.00 and the intensity of the $\text{H}_2\text{-H}_6$ protons are 14.61. The deacetylation of this sample was calculated to be 86.31 %.

$$\text{Acetylation \%} = [(1/3 (1.00) / 1/6 (14.61))] \times 100 = 13.69 \%$$

These calculations were performed for 10 different samples and the data are shown in **Table 2.2**.

Table 2.2 Summary of the Extent of CS Acetylation

Number of CS Samples	Acetylation Percentage of CS
10	14.16 % \pm 5.54

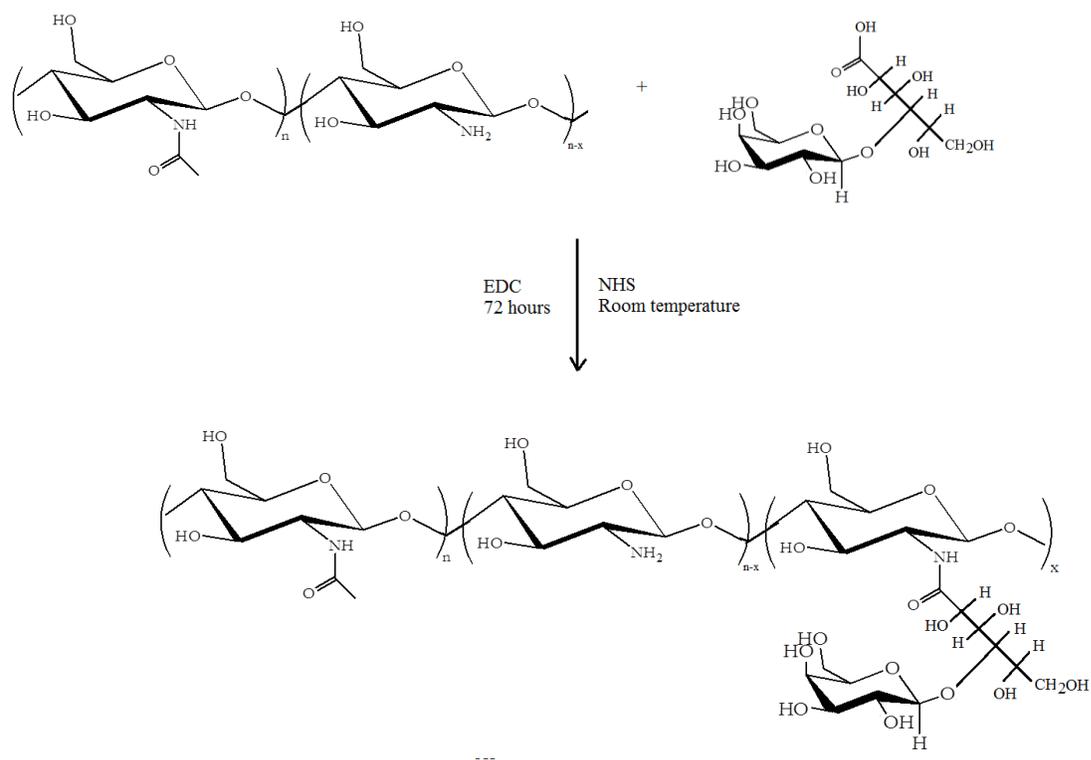


Figure 2.4 Synthesis Scheme of Gal-CS

The synthesis scheme of Gal-CS is shown on **Figure 2.4**. Gal-CS was prepared with EDC, NHS and LA. EDC carbodiimide chemistry has already been used to prepare Gal-CS [77, 78]. EDC is a zero length cross-linker and participates in carboxyl to amine group conjugation. Based upon to this mechanism, Gal-CS was prepared at a pH 5.7-6.0 and the ligand addition was supported by ¹H-NMR and FTIR measurements.

The introduction of LA to CS is an established method for preparing Gal-CS [75, 79-81]. In all of these studies, *N,N,N',N'*-tetramethylethylenediamine (TEMED)/HCl solution was first introduced to the reaction medium, then stirred for 72 h, purified, and finally freeze dried in order to obtain a dry polymer for further experiments. It was observed that TEMED did not contribute to the galactosylation reaction; by contrast, it decreases the galactosylation percentage of the synthesis as shown in **Table 2.3**. Therefore, subsequent syntheses of gal-CS were performed without the addition of TEMED.

Table 2.3 The Effect of TEMED on Galactosylation

CS (mol)	LA (mol)	NHS (mol)	EDC (mol)	TEMED (ml)	Time (days)	Extent of Galactosylation (%)
$6.46 \cdot 10^{-3}$	$6.42 \cdot 10^{-3}$	$1.22 \cdot 10^{-3}$	$3.86 \cdot 10^{-3}$	0.2-0.3	6	≈10 [73]
$1.3 \cdot 10^{-3}$	$5.53 \cdot 10^{-4}$	$2.48 \cdot 10^{-4}$	$7.74 \cdot 10^{-4}$	0	3	≈15

In addition not contributing to the galactosylation synthesis, TEMED causes many other problems. Although TEMED is added at very small amounts, it cannot be removed in the purification process by dialysis alone requiring another method to remove the organic solvent. By not adding TEMED, it is possible to precipitate Gal-CS with acetone as shown in **Figure 2.5**, and the precipitation takes less than 10 min and dries overnight.



Figure 2.5 Precipitation of Gal-CS by Acetone to Show rapid Polymer Precipitation

Gal-CS is characterized by $^1\text{H-NMR}$. The peak at 4.1 ppm is a characteristic peak of LA shown in **Figure 2.6 (A)**. It does not overlap with CS peaks, which are observed at 2.0 ppm and 2.9 to 4.0 ppm. The peaks of LA at 3.4 to 4.0 ppm overlap with the CS backbone peaks. Therefore it is very hard to distinguish LA peaks from CS peaks in this region. Observation of the 4.1 peak in **Figure 2.6 (B and C)** indicates the conjugation of Gal to CS. The extent of galactosylation was calculated according to the intensity ratios of the specific LA peak at 4.1 and the $-\text{CH}_3$ peak of acetyl group of CS at 2.0 ppm. Based upon our previous calculation for deacetylation and, the number and intensity of the $-\text{CH}_3$ peak the extent of galactosylation was calculated.

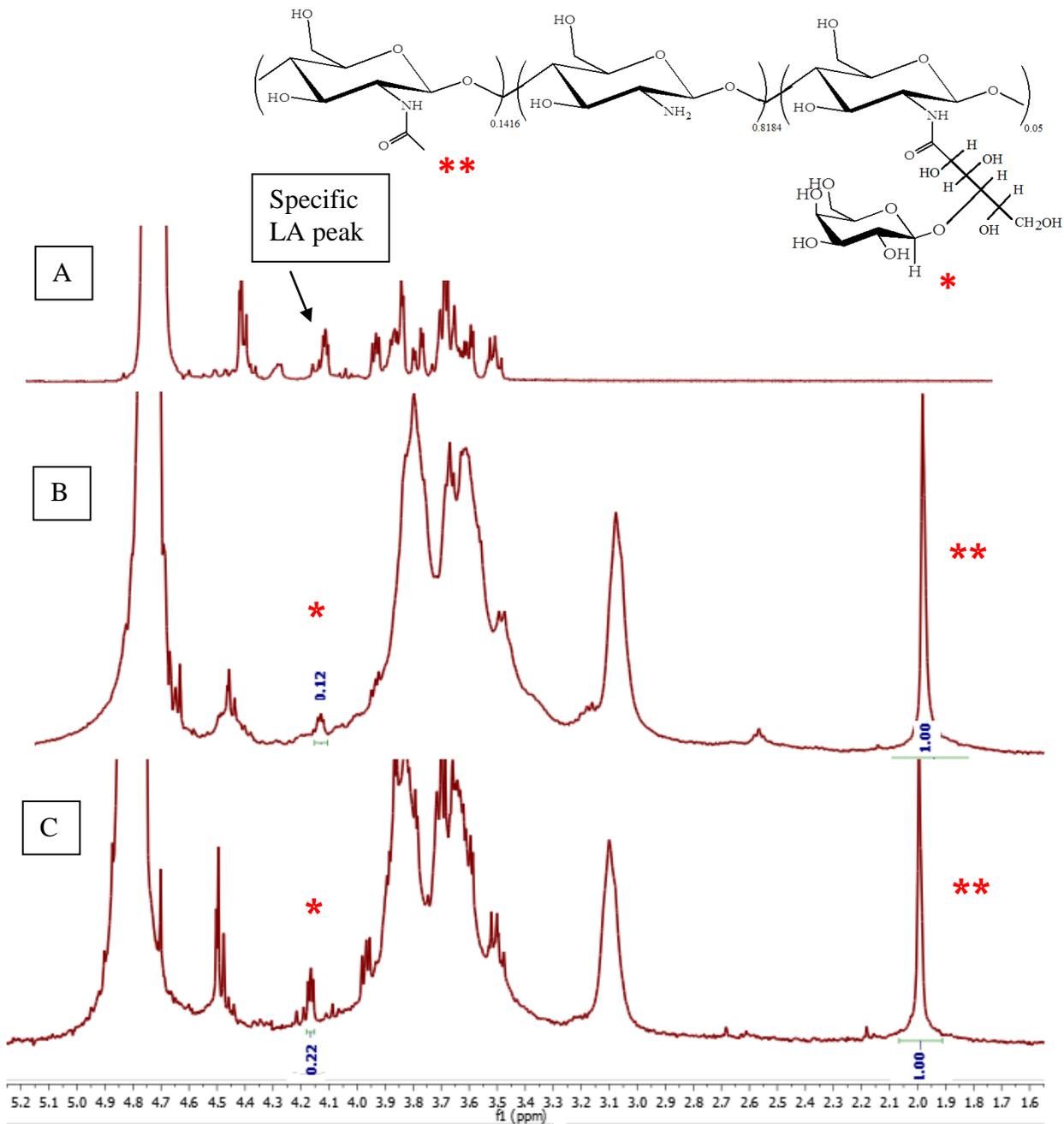


Figure 2.6 400 MHz ^1H NMR Spectrum of LA (A), 5.09 % Gal-CS (B) and 9.34 % Gal-CS (C) in $\text{CF}_3\text{COOD}/\text{D}_2\text{O}$

1.00/3 = 0.333 represents 1 hydrogen of the acetyl peak and this group is present on 14.16 % of the monomers in the chain.

0.3333 → 14.16 %

0.12 → x

x = 5.09 % galactose group

The extent of galactosylation of this polymer is 5.09 % according to the $^1\text{H-NMR}$ spectra. Based on the above calculation method, 5 %, 10 % and 15 % Gal-CS batches were prepared.

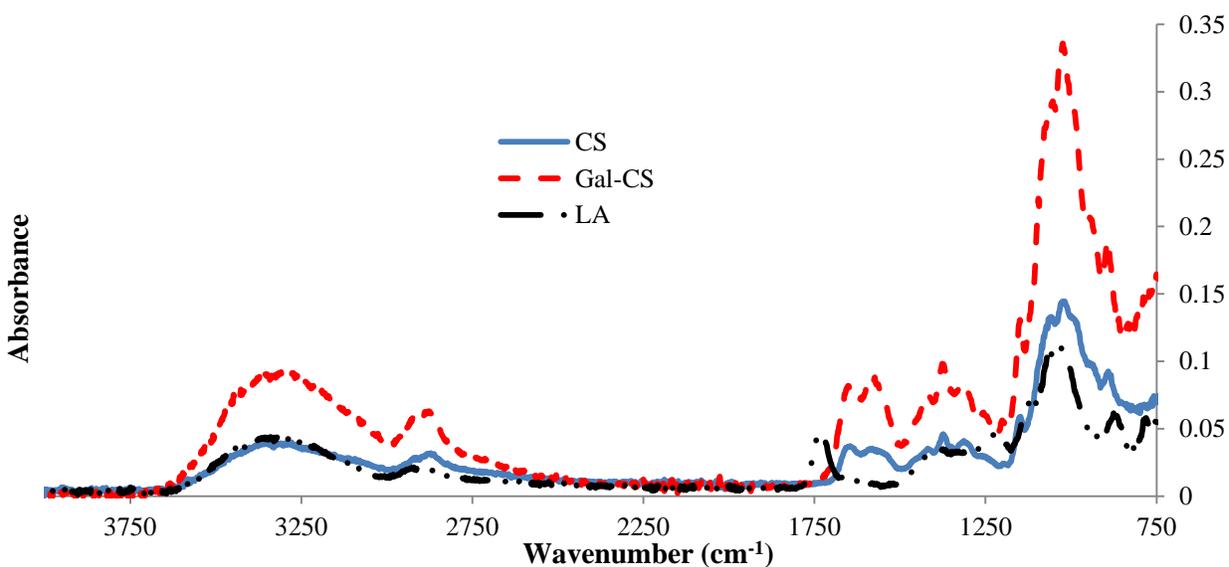


Figure 2.7 FTIR Spectra in the 750 - 4000 cm^{-1} Range for Gal-CS, CS and LA

Figure 2.7 shows the FTIR spectra of CS, Gal-CS and LA. FTIR measurements further indicated the chemical attachment of LA to the primary amine group of CS. A carbonyl group stretching peak of LA is observed at 1712 cm^{-1} but not on the spectrum of Gal-CS. This data shows that the carboxylic acid peak is not present after the galactosylation reaction.

The normalized absorbance values of Gal-CS peaks were compared to the CS peaks and the normalization was based on the $-\text{CH}$ stretching peak at 2850 cm^{-1} . CS has characteristic amide peaks at 1683 cm^{-1} and 1538 cm^{-1} , shown on **Figure 2.7**. In the spectra of Gal-CS, the amide

bands I and II shift were at 1623 cm^{-1} and 1558 cm^{-1} , respectively. Absorbance values of Gal-CS peaks were higher than the CS peaks. Similar trends were observed for the amide II band (N-H), amide I band (C=O), the NH and OH stretching vibrations ($3200\text{-}3500\text{ cm}^{-1}$).

The molecular weights for the repeat units of CS, 5 % Gal-CS and 10 % Gal-CS were calculated. According to this the repeating molecular weight was calculated:

$$203 \times 0.1416 + 161 \times 0.8584 = 166.88\text{ g}$$

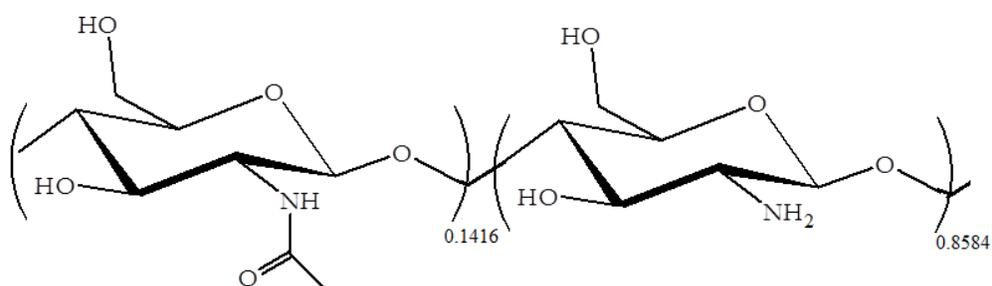


Figure 2.8 CS Repeating Unit Molecular Weight Calculation

The repeating unit molecular weight of 5 % Gal-CS is (Figure 2.9):

$$203 \times 0.1416 + 161 \times 0.8584 + 501 \times 0.05 = 183.88\text{ g}$$

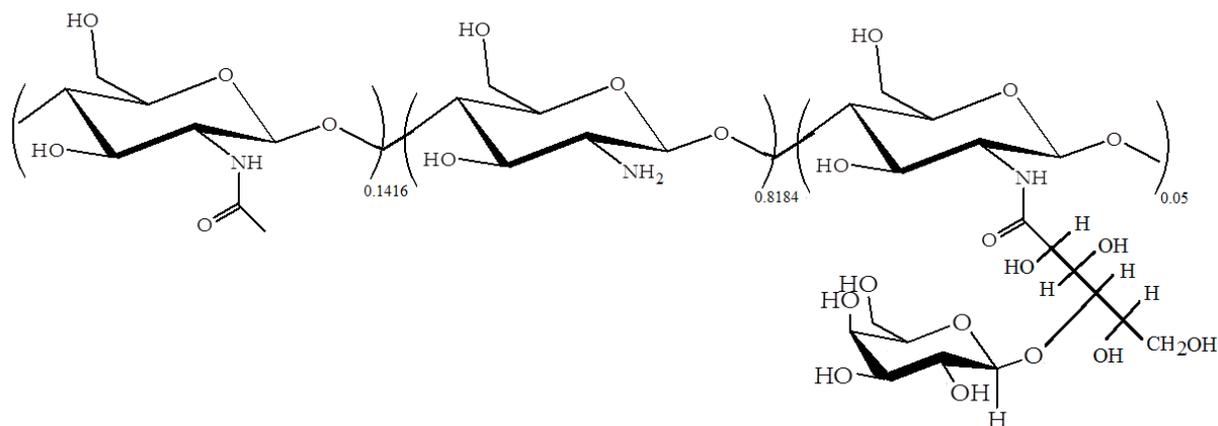


Figure 2.9 5 % Gal-CS Repeating Unit Molecular Weight Calculation

The repeating unit molecular weight of 10 % Gal-CS is (**Figure 2.10**):

$$203 \times 0.1416 + 161 \times 0.7684 + 501 \times 0.10 = 200.88 \text{ g}$$

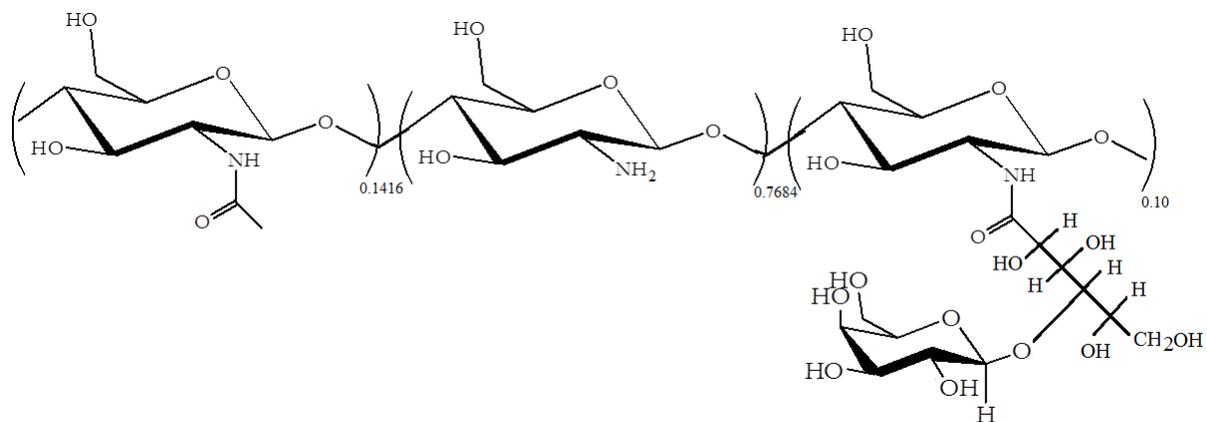


Figure 2.10 10 % Gal-CS Repeating Unit Molecular Weight Calculation

Chapter 3. Assembly of Polyelectrolyte Multilayers with Gal-CS and Accompanying Characterization

3.1 Introduction

The assembly of PEMs is based on the electrostatic attraction between opposite charged PEs. In this study, detachable and free-standing PEMs based on Gal-CS were assembled. In each PEM, up to 10 bilayers of the assembly were comprised of Gal-CS and HA and, subsequent bilayers contained CS and HA.

It was reported that the water content is very high in the polysaccharide based PEMs ranging from 70 - 90 % [82]. HA and CS are highly hydrated polymers, which interacts 20 - 30 water molecules per disaccharide via hydrogen bonds [82]. Boudou et al showed that water content of HA/CS PEMs can reach to 80 % [83]. Therefore the water content of the hydrated CS/HA and Gal-CS/HA/CS PEMs can be ≥ 70 %.

In this study, 50 BL detachable, free-standing Gal-CS/HA/CS PEMs were designed. 5 % and 10 % Gal-CS was used to prepare 5 or 10 BL of 50 BL PEMs. Gal-CS was assembled on one surface.

3.2 Materials and Methods

3.2.1 Materials

Chitosan ($M_w \approx 350$ kDa) and glutaraldehyde (GA) were obtained from Sigma-Aldrich (St. Louis, MO). Hyaluronic acid (HA, $M_w \approx 750$ kDa), and acetic acid were obtained from Fluka (St. Louis, MO). PTFE substrates were obtained from McMaster Carr Supply Company

(Aurora, OH). Phosphate buffered saline (10XPBS; 137 mM NaCl, 2.7 mM KCl, 10 mM Na₂HPO₄) was obtained from Invitrogen Life Technologies (Carlsbad, CA). All other chemicals were received from Fischer Scientific, (Pittsburgh, PA), unless noted otherwise.

3.2.2 Assembly of Detachable and Free-standing PEMs

HA was used as the anionic PE and, CS and Gal-CS were the cationic PEs in the assembly of the detachable PEMs. HA solutions were prepared with 18 MΩ cm Picopure water (hydro, Raleigh NC). CS and Gal-CS solutions were first dissolved in 1 % v/v acetic acid. The solution concentrations of CS and HA were 2 mM and 1 mM for 50 bilayer PEMs, and 10 mM and 5 mM for 15 BL PEMs respectively. The solution concentrations were calculated based upon the repeat unit molecular weight of the polymer, 166.88 g mol⁻¹ for CS and 874.7 g mol⁻¹ for HA. The solution concentrations of 5 % Gal-CS are 1.89 mM and 9.2 mM for the 50 bilayer and 15 bilayer solutions, respectively. The solution concentrations of 10 % Gal-CS are 1.7 mM and 8.5 mM for the 50 bilayer and 15 bilayer solutions, respectively. The molecular weights of the 5 % and 10 % Gal-CS are 183.88 g mol⁻¹ and 200.88 g mol⁻¹. The solutions were filtered through a 0.45 μm polyethersulfone filters (Nalgene, Rochester NY). The pKa value of HA is about 3.0 [84] and pKa of CS is 6.5 [85].

The pH of the solutions was 4.0 for HA, 5.0 for CS and Gal-CS, and 4.5 for water in the 50 BL PEMs preparation. The PEMs were assembled on inert hydrophobic PTFE substrates by using a robotic deposition system (NanoStrata, Gainesville, FL). The PTFE substrates were cleaned by sonication in toluene for 1 hour. The hydrophobicity of the clean substrates was measured by using static water contact angle measurements (KSV Instruments, Helsinki, Finland). The

average contact angle was $111.35 \pm 3.1^\circ$ (averaged over 3 different samples, around 30 different measurements per sample). PEMs with different properties were prepared by varying polymer deposition time, polymer concentrations, pH of solutions and cross-linking conditions. The preparation of PEMs started with the deposition of the negative PE, HA followed by the cationic PE (CS or Gal-CS), alternately. After each deposition, the assembly was rinsed in water for 4 min. One bilayer is composed of one anionic and one cationic PE. 50 and 15 bilayer detachable PEMs were prepared with different deposition times such as 20 min, 40 min or 50 min. After that, PEMs were dried at room temperature overnight and detached from the underlying surface. PEMs that did not detach from the substrate were denoted as “un-detachable” and those with tears were noted as “cracks appeared”. PEMs were cross-linked with either 4 w/v % or 8 w/v % GA. The range for the exposure time to the cross-linker was 20 sec to 40 sec for 15 BL PEMs and 1 min to 2 min for 50 BL PEMs. PEMs were washed with water for 2 days and dried at room temperature overnight. These PEMs will be named “washed PEMs” in the subsequent sections. PEMs were kept at room temperature until further use and detached prior to experimentation.

3.2.3 Aqueous Stability of PEMs

Detachable 50 BL Gal-CS/HA/CS PEMs were peeled from the substrate and weighed. After that they were placed in 1XPBS at 37°C and up to 7 days. After 7 days, PEMs were rinsed with DI water and dried at 50°C for 4 days under vacuum. The weight of the sample, before and after incubation to PBS was obtained.

3.2.4 Thickness Measurements

A profilometer (Veeco Dektak 150, Veeco Metrology, Santa Barbara, CA) was used to measure the thickness on the PEMs. 9 measurements were obtained per sample at dry conditions at a scan length of 1000 μm .

3.2.5 Optical Properties

The optical properties of PEMs were measured on a UV/vis spectrophotometer (Perkin Elmer Lambda 25, Downers Grove IL) between 400 - 900 nm. The optical transparencies of both dry and hydrated PEMs were measured.

3.2.6 Atomic Force Microscopy (AFM)

The surface topography of the detachable PEMs was measured with AFM (Veeco Multimode AFM, Santa Barbara CA). Silicon nitride DNP tips with a spring constant of 0.12 N/m (Veeco, Santa Barbara CA) were used in contact mode at a scanning rate of 2 Hz. The data was analyzed by using Nanoscope software (Veeco, Santa Barbara CA) to determine the surface roughness of PEMs.

3.3 Results

Anionic PE (HA) and cationic PEs (Gal-CS and CS) were sequentially assembled on clean, inert and hydrophobic PTFE substrates. The detachability of PEMs was dependent on the concentration of the PE solutions, PE deposition time, total number of bilayers, galactosylation percentage and, the number of bilayers that contained Gal-CS. The ease of detachment increased as the total number bilayers, concentration of the solutions and deposition time of PE was higher.

3.3.1 Results of 50 BL PEMs

50 BL free standing detachable CS/HA PEMs were previously prepared in our group at 8 w/v % GA for 1 min and 2 min [10]. These PEMs were modified with 5 % and 10 % Gal-CS at the conditions shown in **Table 3.1**. The galactosylated polymer is assembled on the substrate side of the PEMs for each multilayer. The substrate side of the PEMs indicates the side of the PEM in contact with the PTFE substrate and the air-side denotes the side of PEMs in contact with air (**Figure 3.2**).

Table 3.1 Conditions of Washed, Detachable 50 bilayer PEMs with 20 min Deposition Time, [HA] = 1 mM, [CS] = 2 mM, [Gal-CS] = 1.8 mM

Extent of galactosylation (%)	Number of BL with Gal-CS	Cross-linking condition (w/v)	Detachable
5	5	Un-modified	Yes
5	5	1 min 4 % GA	Yes
5	5	2 min 4 % GA	Yes
5	5	1 min 8 % GA	Yes
5	5	2 min 8 % GA	Yes
5	10	Un-modified	Yes
5	10	1 min 4 % GA	Yes
5	10	2 min 4 % GA	Yes
5	10	1 min 8 % GA	Yes
5	10	2 min 8 % GA	Yes
10	5	Un-modified	Yes
10	5	1 min 4 % GA	Yes
10	5	2 min 4 % GA	Yes
10	5	1 min 8 % GA	Yes
10	5	2 min 8 % GA	Yes
10	10	Un-modified	Yes
10	10	1 min 4 % GA	Yes
10	10	2 min 4 % GA	Yes
10	10	1 min 8 % GA	No
10	10	2 min 8 % GA	No

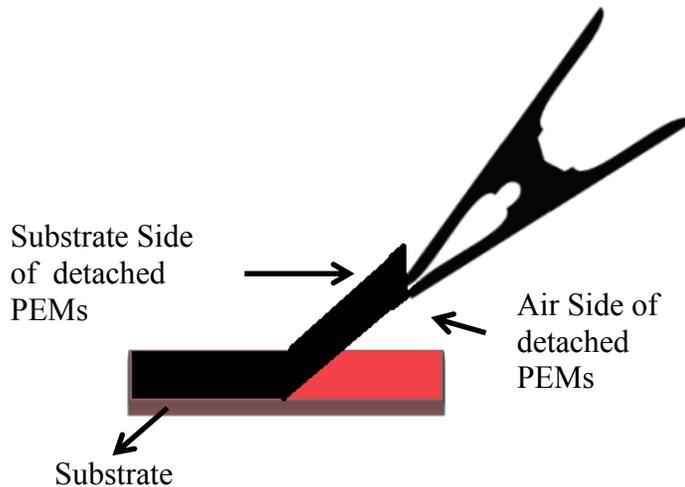


Figure 3.1 Schematic to Show the Surface and Air Side of the PEMs

5 % and 10 % Gal-CS PEMs were cross-linked with 4 w/v % and 8 w/v % GA for 1 and 2 min. GA increases the rigidity of the PEMs, however it is a known cytotoxin [86]. To be able to use the PEMs for biological application, it is necessary to remove GA by washing. In this study, methods, cross-linked PEMs were rinsed in DI water for 2 days. Four different cross-linking conditions of PEMs were tested for this study to investigate the effects of cross-linking on mechanical properties and cellular responses. These effects have not been investigated in this study and will be the focus of future investigations.

PEMs with 10 BL 10 % Gal-CS cross-linked with 8 w/v % GA were not detachable (**Table 3.1**). On the other hand, PEMs with 5 % Gal-CS and 5 BL 10 % Gal-CS/HA/CS PEMs were detachable.

Figure 3.2 shows 50 BL PEMs assembled with Gal-CS/HA/CS.



Figure 3.2 (A) Assembly of 50 BL Gal-CS/HA/CS PEMs and (B) a detached 50 BL PEMs which includes 5 BL of 5 % Gal-CS

The aqueous stability is important for biological applications. PEMs that are not cross-linked degrade within 5min when placed in 1XPBS. Cross-linked PEMs with 4 w/v % and 8 w/v % GA for 1 or 2 min were monitored over a period of 7 days. According to the results presented in **Figure 3.3**, the weight retention over a seven day period is more than 90 % in the PEMs assembled with 5 bilayers of 5 % Gal-CS/HA/CS cross-linked with 8 w/v % and 4 w/v % GA. The weight retention percentage is 82.6 ± 6.4 , 94.3 ± 2.2 , 96.4 ± 1.9 and 96.9 ± 2.6 for 4 w/v % GA for 1 min and 2 min and 8 % w/v GA 1 min and 2 min conditions respectively. Since the weight loss was more than 10 % in 5 % Gal-CS 5 bilayer 4 w/v % GA 1 min cross-linked condition, this PEM was not considered for further experimentation.

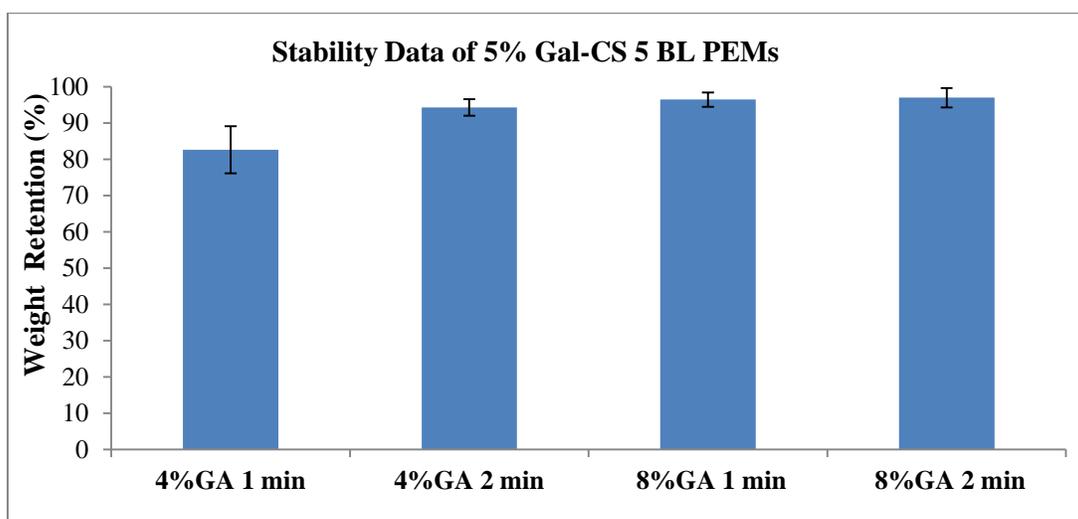


Figure 3.3 Stability Data of 50 BL 5 % Gal-CS PEMs with 20 min Deposition (n=3)

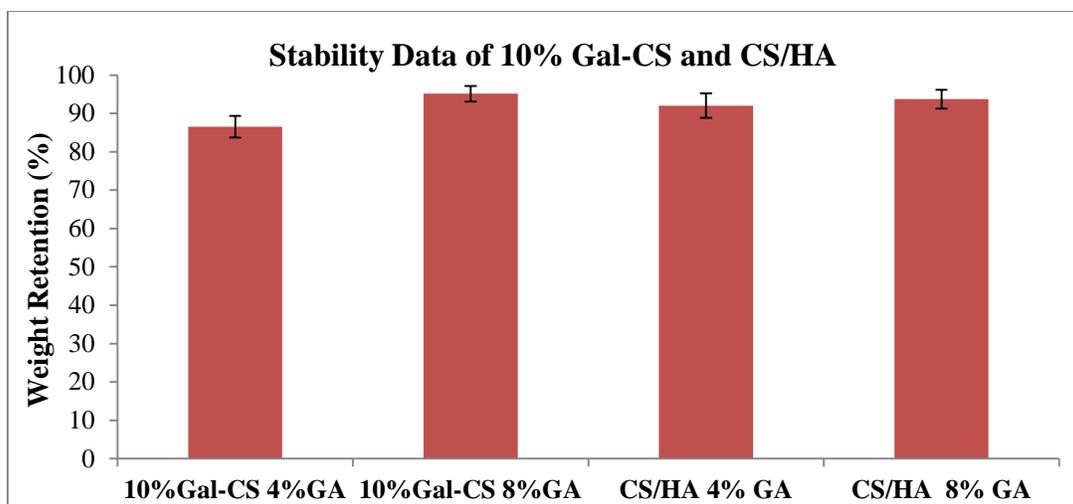


Figure 3.4 Stability Data of 50 BL 10 % Gal-CS and CS/HA PEMs with 20 min Deposition, Cross-linked for 2 min (n=3)

The stability data of 10 % Gal-CS/HA/CS and CS/HA PEMs cross-linked with 4 w/v and 8 w/v % GA for 2 min is shown in **Figure 3.4**. Briefly, weight retention percentage of the 10 % Gal-CS/HA/CS PEMs 4 w/v % and 8 w/v % GA and CS/HA 4 w/v % and 8 w/v % GA cross-linking conditions are 86.54 ± 2.81 , 95.12 ± 2.1 , 92.01 ± 3.1 and 93.7 ± 2.42 respectively.

The thickness of 50 BL dry PEMs, where 5 BLs were prepared with 5 % or 10 % Gal-CS were measured by profilometry. The results are shown in **Table 3.2** and **Table 3.3**.

Table 3.2 Thickness of dry 5 BL 5 % Gal-CS/HA/CS PEMs, Total Number of BL 50 (n=9)

1 min 4 w/v % GA (nm)	2 min 4 w/v % GA (nm)	1 min 8 w/v % GA (nm)	2 min 8 w/v % GA (nm)
2329 ± 69	2702 ± 31	2585 ± 14	2804 ± 28

Table 3.3 Thickness of dry 5 BL 10 % Gal-CS/HA/CS PEMs, Total number of BL 50 (n=9)

2 min 4 w/v % GA (nm)	2 min 8 w/v % GA (nm)
2380 ± 81	2392 ± 110

UV-transmission of the PEMs was measured to determine their optical transparency. Measurements were taken in the visible light range of 400 to 900 nm. Transmission of hydrated and dry samples was measured for unmodified samples and samples at different cross-linking conditions. In the dry state, the transmission of 10 % 5 BL Gal-CS/HA/CS PEMs (unmodified or cross-linked) was between 61 – 66 % and the transmission of 10 % 10 BL Gal-CS/HA/CS PEMs (unmodified or cross-linked) was 50 – 70 %. In the hydrated state, the transmission of 10 % 5 BL Gal-CS/HA/CS PEMs (unmodified or cross-linked) was between 94 – 97 % as shown in **Figure 3.5** and **Figure 3.6** and for 10 BL PEMs the range was 93 – 98 % as shown in **Figure 3.7**. According to these data, all PEMs have transmission higher than 95 % in the hydrated state. The decrease observed at lower wavelengths in the percent transmission can be attributed to scattering (**Figure 3.5**, **Figure 3.6** and **Figure 3.7**).

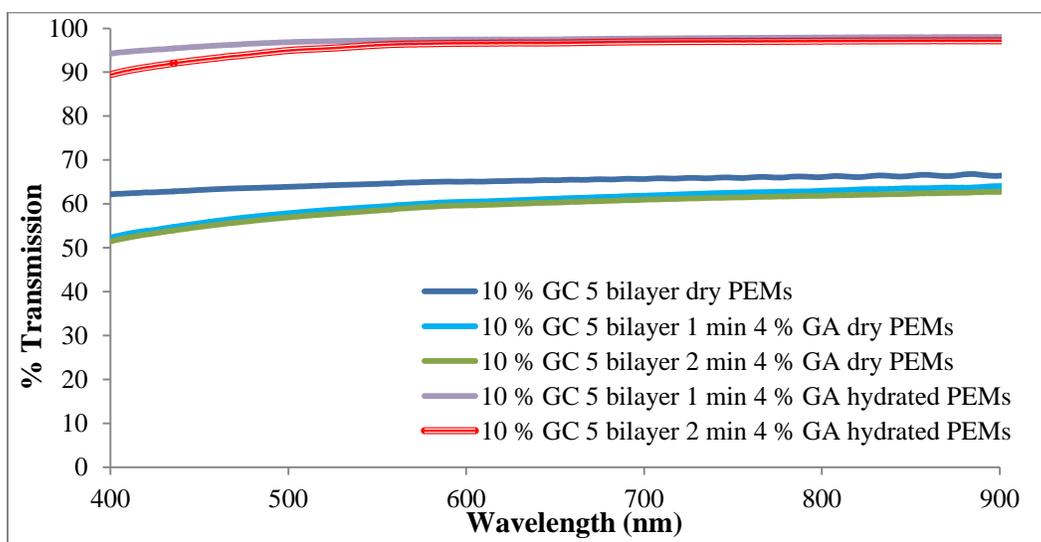


Figure 3.5 Optical Transmission in the 400 – 900 nm Range for the Dry and Hydrated 50 BL PEMs, 5 BL Prepared with 10 % Gal-CS and Cross-linked with 4 w/v % GA

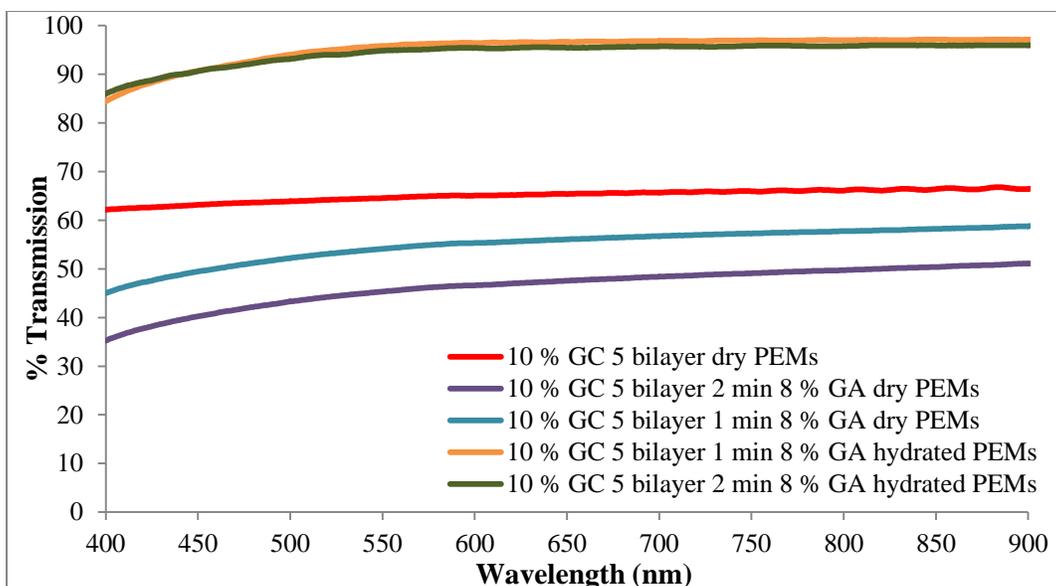


Figure 3.6 Optical Transmission in the 400 – 900 nm Range for the Dry and Hydrated 50 BL PEMs, 5 BL Prepared with 10 % Gal-CS and Cross-linked with 8 w/v % GA

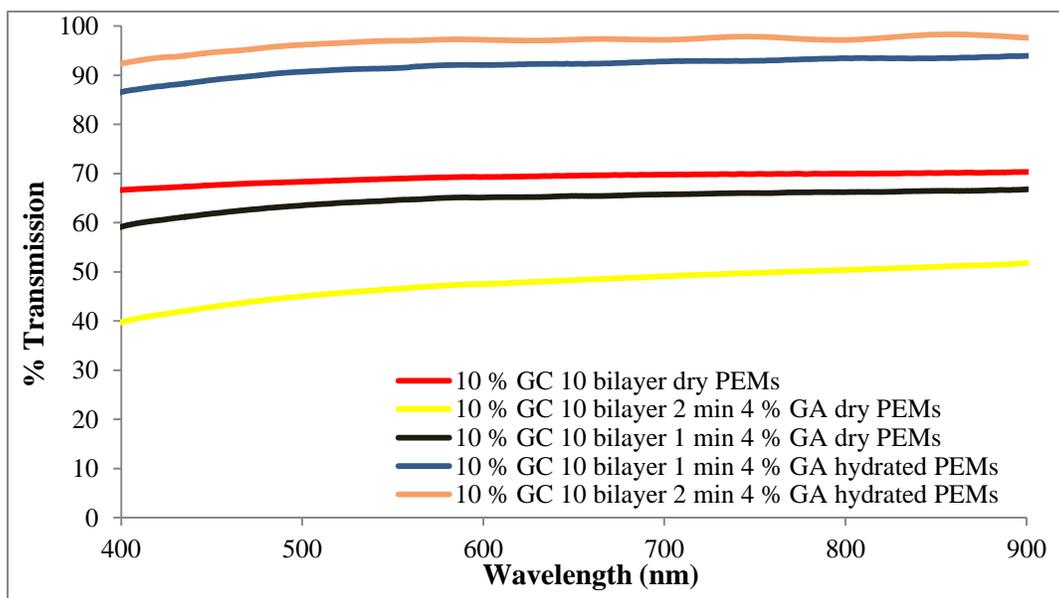


Figure 3.7 Optical Transmission in the 400 – 900 nm Range for the Dry and Hydrated 10 BL PEMs, 10 BL Prepared with 10 % Gal-CS and Cross-linked with 4 w/v % GA

The surface topographies of 5 % Gal-CS/HA/CS PEMs and CS/HA PEMs at 4 w/v % GA for 2 min and 8 % w/v GA for 2 min cross-linking conditions were measured to determine roughness.

The surface topography of the air side of the 5 % Gal-CS/HA/CS PEMs was investigated using AFM and the images are presented in **Figure 3.8**. No significant changes were observed as a result of Gal-CS (**Figure 3.9**). The substrate side roughness of 4 % and 8 % GA cross-linked 5 % Gal-CS PEMs are 1.94 ± 0.55 nm and 2.25 ± 0.09 nm, respectively. The substrate side roughness of 4 % and 8 % GA cross-linked CS PEMs are 1.66 ± 0.05 nm and 2.3 ± 0.62 nm, respectively. The air side roughness of 4 % and 8 % GA cross-linked 5 % Gal-CS PEMs are 4.04 ± 2.09 nm and 4.3 ± 1.51 nm, respectively.

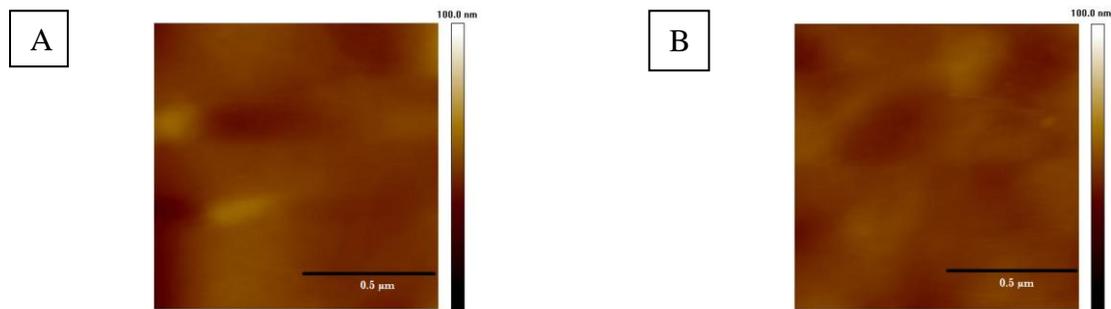


Figure 3.8 Air Side AFM Images of 50 BL 20 min Deposition PEMs 5 BL 5 % Gal-CS /HA/CS PEMs: A) Cross-linked with 8 w/v % GA for 2 min, B) Cross-linked with 4 w/v % GA for 2 min

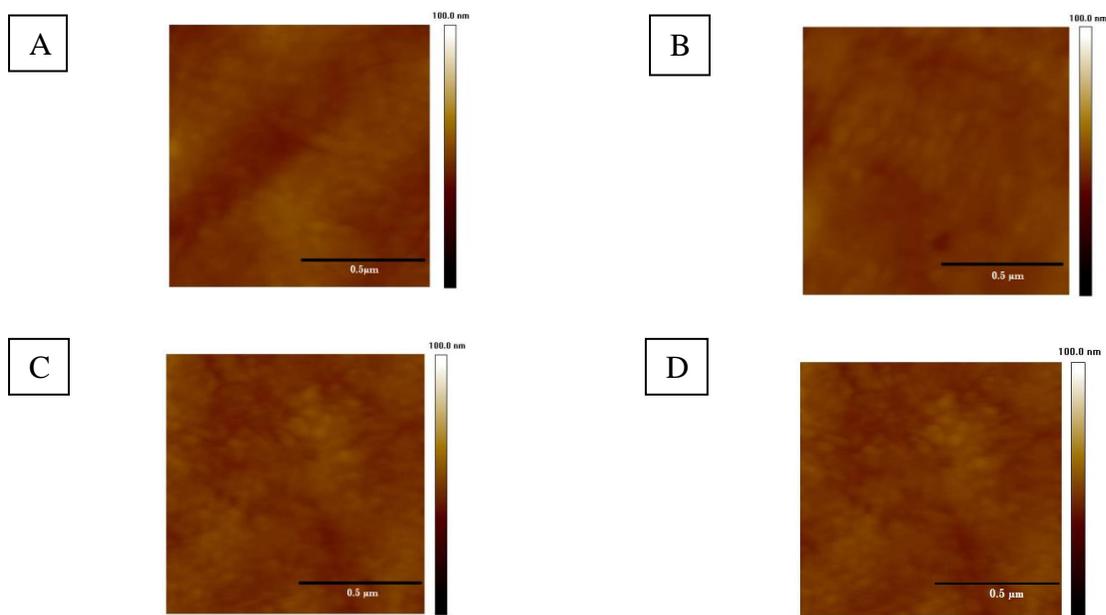


Figure 3.9 Substrate Side AFM Images of 50 BL 20 min Deposition PEMs: A) 5 BL 5 % Gal-CS/HA/CS PEMs Cross-linked with 8 w/v % GA for 2 min, B) 5 BL 5 % Gal-CS/HA/CS PEMs Cross-linked with 4 w/v % GA for 2 min C) CS/HA PEMs Cross-linked with 8 w/v % GA for 2 min D) CS/HA PEMs Cross-linked with 4 w/v % GA for 2 min

3.3.2 Results of 15 BL PEMs

15 BL free standing detachable Gal-CS/HA/CS PEMs were prepared with 8 w/v % GA 30 sec crosslinking condition. The aim of this study was to prepare thin PEMs, whose thickness will be within the range of 500 - 1000 nm under hydrated conditions. The assembly conditions of 5 % and 10 % Gal-CS PEMs are shown in **Table 3.4**. The galactosylated polymer is assembled on the substrate side of the PEMs. The optimum conditions for 15 BL 5 % and 10 % Gal-CS PEMs are obtained with 50 min deposition time, and pH of the Gal-CS, HA, water and CS solutions were 4.0, 4.0, 4.0 and 5.0 respectively. 15 BL PEMs were cross-linked with 8 w/v % GA for 30 sec. 15 BL CS/HA PEMs were also prepared at the same conditions to be compared with the Gal-CS/HA/CS PEMs and the CS/HA PEMs were robust and detachable.

A

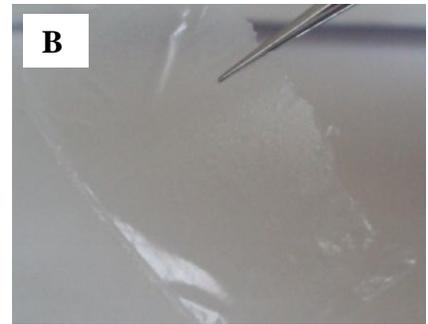


Figure 3.10 (A) Illustration of 15 BL Gal-CS/HA/CS PEMs on Substrate and (B) a picture of detached 15 BL PEMs includes 2.5 BL of 5 % Gal-CS/HA/CS

Table 3.4 Assembly Conditions of Washed, Detachable and Free-standing 15 BL Gal-CS/HA/CS PEMs

Deposition Time (min)	Extent of galactosylation (%)	Number of layers with Gal-CS	pH of Gal-CS solution	pH of HA solution	pH of CS solution	pH of Water	Crosslinking Time with 8 w/v % GA (sec)	Detachability
50	5	5	4	4	5	4	-	Yes
50	5	5	4	4	5	4	20	Yes, but not robust
50	5	5	4	4	5	4	30	Yes, robust
50	5	5	4	4	5	4	40	Yes, robust
50	10	5	4	4	5	4	-	Yes
50	10	5	4	4	5	4	30	Yes, robust
50	-	-	-	4	5	4	30	Yes, robust

Chapter 4. Summary

4.1 Discussion and Conclusions

15 BL and 50 BL detachable and free-standing Gal-CS/HA/CS PEMs were prepared using the layer by layer method. The aim of the addition of galactose group to the PEMs was to promote the adhesion of hepatocytes.

50 BL free-standing detachable PEMs were fabricated and characterized at different cross-linking conditions. These PEMs contained either 5 BL or 10 BL of Gal-CS (5 % or 10 % galactosylation). They exhibited over 90 % weight retention after they were maintained at 37 °C for 7 days. According to the optical transmission data, PEMs have greater than 90 % transparency under hydrated conditions. PEMs have a smooth surface. The substrate side roughness of 4 % and 8 % GA cross-linked 5 % Gal-CS PEMs are 1.94 ± 2.51 nm and 2.25 ± 2.85 nm, respectively. The substrate side roughness of 4 % and 8 % GA cross-linked CS PEMs are 1.66 ± 2.15 nm and 2.3 ± 2.8 nm, respectively. The air side roughness of 4 % and 8 % GA cross-linked 5 % Gal-CS PEMs are 4.04 ± 5.03 nm and 4.3 ± 5.68 , respectively.

4.2 Future Studies

In the future, PEMs containing Gal-CS can be used in hepatic tissue engineering applications. The cellular responses to the PEMs such as cytotoxicity and markers for hepatic functions can be investigated. In addition, the presence and localization of ASGP-R can be imaged using conventional immunostaining procedures. PEMs can be chemically modified with other ligands to promote adhesion with other hepatic cell types such as LSECs. The tri-peptide arginine-

glycine-aspartic acid (RGD) is a potential ligand for such an application since it can bind to integrins on LSECs.

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